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1. Introduction

Hydrogels, cross-linked polymer networks containing water, are expected to be applied for biomaterials such as artificial cartilage, vessels, and prosthetic joints due to their high water content and biocompatibility.¹ For the applications as biomaterials, the mechanical toughness of polymer gels is not enough and needs to be improved. The reason for the brittleness of polymer gels is the heterogeneous strain distribution caused by their inhomogeneous network structure.^{2,3} When a polymer gel is stretched, local stress concentrates on short strands between cross-links. The stress-concentrated strands are highly stretched and become potential fracture onsets, which dominate the macroscopic fracture properties of polymer gels. The stress concentration under deformation can be visualized by the introduction of mechanically responsive

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Quasi-elastic neutron scattering study on dynamics of polymer gels with controlled inhomogeneity under uniaxial deformation

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We study the segmental and monomer dynamics of polymer gels with controlled inhomogeneity under uniaxial deformation by means of quasi-elastic neutron scattering (QENS). In order to clarify the effect of the homogeneity of a network structure on the polymer dynamics in gels, we compare two types of polymer gels with controlled homogeneity: a homogeneous tetra-PEG gel (homo-gel) prepared from uniform tetra-arm pre-polymers and a heterogeneous tetra-PEG gel (hetero-gel) with a small amount of shorter tetra-PEG pre-polymer. The different inhomogeneity in the homo-gel and the hetero-gel has little effect on the average relaxation time of the chain dynamics in the undeformed state. The difference in the local dynamics in the gels is emphasized under uniaxial deformation: while the homogel shows a single relaxation mode, the hetero-gel exhibits a bimodal distribution of relaxation times with a slow dynamic mode ascribed to highly stretched short strands, which causes a more brittle macroscopic fracture compared with that in the case of the homo-gel.

chemical groups, mechanophores, into polymer networks.^{4–6} The mechanophores emit light in response to applied force, and serve as molecular sensors to detect the stress concentration in deformed polymeric materials. However, the complexity of the synthesis procedures for the mechanophores and their miscibility with polymer matrices limit their broad application to polymeric materials.

Here, we focus on the molecular dynamics of polymer chains to detect the strain distribution in polymer networks without adding any probes. Polymer chains exhibit hierarchical dynamics on various time and spatial scales: cooperative diffusion of polymer networks, the Rouse/Zimm mode corresponding to the dynamics of connected segments, and the monomer diffusion mode.^{7–21} The segment and monomer dynamics in cross-linked polymer gels in an un-deformed state have been studied by quasielastic neutron scattering (QENS) techniques.^{9–21} However, to the best of our knowledge, the segment/monomer dynamics in deformed polymer gels have not been observed yet.

In this study, the segment/monomer dynamics of polymer gels under uniaxial deformation is investigated by means of QENS. In order to clarify the effect of heterogeneity in a polymer network structure, we prepared two types of polymer gels with controlled heterogeneities: a homogeneous tetra-PEG gel prepared by end-cross-linking of tetra-arm prepolymers (homogel),²² and a heterogeneous tetra-PEG gel (hetero-gel) containing a small amount of tetra-PEG prepolymers with shorter arms.²³ The hetero-gel shows a more brittle fracture behavior than the

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homo-gel, which suggests that a stress-concentration occurs in hetero-gel under deformation. From the QENS results, we demonstrate how the homogeneity of the network structure affects the segment/monomer dynamics of polymer gels in the un-deformed and stretched states. The hetero-gel exhibits an elastic component in its dynamic scattering factor, which corresponds to the slow dynamics of highly stretched strands and is the molecular origin of the brittleness of the polymer gel.

2. Experimental section

2.1 Sample preparation

We prepared the tetra-PEG gel by end-crosslinking of *N*-hydroxysuccinimide (NHS)-terminated tetra-PEG and amino-terminated tetra-PEG. The homogeneous tetra-PEG gel, homo-gel (Fig. 1(a)), was fabricated by using NHS-terminated and amino-terminated tetra-PEGs with the same total molecular weight, 20k (SUNB-RIGHT PTE-200HS and PTE-200PA, NOF Corporation (Tokyo, Japan)). The heterogeneous tetra-PEG gel, hetero-gel (Fig. 1(b)), was prepared from PTE-200HS, PTE-200PA, and amino-terminated tetra-PEG with a smaller total molecular weight, 5k (SUNBRIGHT PTE-50PA, NOF Corporation (Tokyo, Japan)).²³ The strand length in the hetero-gel is not uniform, but bimodal.

For the homo-gel, the two tetra-PEGs, PTE-200PA and PTE-200HS, were dissolved separately in 0.1 M phosphate buffer (pH = 7.0) with a polymer concentration of 10 wt%. The phosphate buffer was prepared by mixing disodium phosphate, phosphoric anhydride, and sodium hydrogen anhydrate in D₂O. The two solutions of PTE-200PA and PTE-200HS were mixed and injected into a mold, and were left to stand for a day to proceed with the gelation reaction. Finally, we obtained a sheet of the hetero-gel with 1 mm thickness. The hetero-gel was prepared from PTE-200HS and PTE-200PA/PTE-50PA solutions.



Also, as a reference, we prepared tetra-PEG solutions with the same compositions as those of the tetra-PEG gels (homo-gel and hetero-gel). For a comparison with the homo-gel and heterogel, we prepared 10 wt% PTE-200HS solution and PTE-200PA/ PTE-50PA solution, respectively. The solvent of both the solutions was 0.1 M deuterated phosphate buffer. In the PTE-200PA/PTE-50PA solution, the concentrations of PTE-200PA and PTE-50PA were 8.75 wt% and 1.25 wt%, respectively.

2.2 Uniaxial tensile test

Uniaxial tensile tests on homo-gel and hetero-gel were performed on a mechanical testing apparatus (EZ-S-500N, SHIMADZU, Kyoto, Japan). For the tensile tests, we used stripe-shaped gel specimens with 1 mm thickness and 3 mm width. The initial gap between cramps was 20 mm. The cross-head speed was set as 50 mm min⁻¹.

2.3 Quasi-elastic neutron scattering

For QENS measurements of un-deformed homo-gel and heterogel, we prepared gel sheets (40 mm \times 42 mm \times 1 mm) and covered them with aluminum foils. The gel sheets were put into aluminum cylinder cells having 14 mm inner diameter and 0.25 mm thickness. For the QENS experiments of the stretched tetra-PEG gels (homo-gel and hetero-gel), the gel sheets were cut into smaller specimens (10 mm \times 20 mm \times 1 mm for extension ratio $\lambda = 2$ and 10 mm \times 13 mm \times 1 mm for $\lambda = 3$). Each specimen was stretched with hands to a length of 40 mm, and the strain was maintained by fixing the edges of the specimen on an aluminum foil via an epoxy adhesive. For each extension ratio, 4 specimens were attached on the aluminum foil. The stretched gel specimens were set in a 2 mm gap of concentric double cylinder aluminum cells having 14 mm inner diameter of the outer cylinder and 10 mm outer diameter of the inner cylinder. In order to avoid the scattering from the adhesives, the top and bottom parts of the cells were covered with cadmium sheets. The tetra-PEG solutions were set into a 1 mm gap of concentric double cylinder aluminum cells having 14 mm inner diameter of the outer cylinder and 12 mm outer diameter of the inner cylinder. All the aluminum cells were sealed with indium wire.

The QENS measurements were conducted using a time-offlight near-backscattering spectrometer DNA BL02, at the Materials and Life Science Experimental Facility (MLF) at the Japan Proton Accelerator Research Complex (J-PARC) in Ibaraki, Japan.^{24,25} The energy resolution was 2.8 and 3.6 μ eV for gels and solutions, respectively, and the energy transfer ranged from -0.02 to 0.1 meV. The incident neutron beam and scattering vector were perpendicular to the stretching direction of the gels as shown in Fig. 2. The covered angle of the Si(111) plane analyzed was from -14 to 21° and from -30 to 138° in vertical



Fig. 1 Schematic illustrations of (a) homo-gel and (b) hetero-gel.

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Fig. 2 (a) Schematic illustration of stretching gels. (b) Schematic illustration of the experimental setup for QENS measurements of stretched gels.

and horizontal directions, respectively. The amplitude of the scattering vector, Q, was in the range of 0.125 to 1.825 Å⁻¹. Each measurement was carried out at 300 K for 6 hours with 500 kW proton beam power. The data were circular averaged in the data reduction. To extract the dynamics of the solute, the scattering from the solvent was removed by subtraction based on the volume fraction.

3. Results and discussion

3.1 Tensile tests

Fig. 3 shows the stress–extension ratio $(\sigma - \lambda)$ curves of homogel and hetero-gel. Young's moduli of homo-gel and hetero-gel are 49 kPa and 50 kPa, respectively, which suggests that the average network densities in these two gels are almost the same.²³ However, the hetero-gel fractures at an extension ratio $\lambda = 4.5$, while the homo-gel can be stretched up to $\lambda = 7$. Since the hetero-gel contained short tetra-PEG, the network structure was heterogeneous compared with that of the homo-gel. This heterogeneity of the network structure causes stress concentration on the short strands under stretching and a lower strain at break for the hetero-gel. This result is consistent with that of the previous work on bimodal tetra-PEG gels.²³

3.2 Effects of gelation on polymer dynamics

The effect of gelation on polymer chain dynamics was studied by comparing QENS results of the tetra-PEG solutions and gels.



Fig. 3 Stress-extension ratio curves of the homo-gel and hetero-gel.

Fig. 4(a) shows dynamic structure factors $S(Q, \omega)$ of the tetra-PEG precursor solutions and gels at Q = 0.35 Å⁻¹. Both homoand hetero-gels show no elastic component attributed to slow dynamics compared to energy resolution. The dynamic structure factors were fitted using the KWW function:

$$S(Q,\omega) = \left\{ \operatorname{FT}\left[A \exp\left(-\left(\frac{t}{\tau}\right)^{\beta}\right)\right] \right\} \otimes R(Q,\omega)$$
(1)

where τ is the relaxation time, β is the stretching exponent corresponding to the distribution of τ , *A* is the amplitude of the relaxation mode, FT is the Fourier transform, and $R(Q, \omega)$ is the resolution function. The data of vanadium was utilized for the resolution function. As shown by dashed lines in Fig. 4(a), the measured $S(Q, \omega)$'s fitted well with Eqn (1). From the obtained τ and β , the average relaxation time τ can be calculated as follows:

$$\langle \tau \rangle = \frac{\tau}{\beta} \Gamma\left(\frac{1}{\beta}\right) \tag{2}$$

where Γ is the gamma function. Fig. 4(b) shows the *Q* dependence of τ for the tetra-PEG solutions and gels. For all the samples, in the lower Q regime (Q < 0.5 Å⁻¹), τ is proportional to Q^{-3} corresponding to Zimm dynamics, while τ decays as Q^{-2} reflecting the monomer diffusion mode for $Q > 0.5 \text{ Å}^{-1}$. Homo-gel and hetero-gel show almost the same τ , suggesting that the degree of inhomogeneity in the network structure does not influence the segment/ monomer dynamics of the polymer networks in the un-deformed state. This is consistent with the homogeneous network structure of the tetra-PEG gels confirmed by previous small-angle neutron scattering (SANS) and neutron spin echo (NSE) studies. 19,26,27 Fig. 4(c) shows the Q dependence of β for the tetra-PEG gels and solutions. In the case of tetra-PEG solutions, β for $Q > 0.5 \text{ Å}^{-1}$ is about 0.9 close to 1 corresponding to the monomer diffusion with a single relaxation mode, while β in the low-Q regime (Q < 0.5 Å⁻¹) is around 0.8 and the deviation from 1 is ascribed to the non-Brownian Zimm dynamics. Compared with the tetra-PEG solutions, the cross-linked gels show lower β . At lower Q below 0.5 Å⁻¹ where Zimm dynamics was observed, β of homo- and hetero-gels was close



Fig. 4 (a) Dynamic structure factors $S(Q,\omega)$ at Q = 0.35 Å⁻¹, (b) Q dependence of average relaxation time τ and (c) Q dependence of stretching exponent β for the tetra-PEG gels and solutions.



3.3 Effects of stretching on polymer dynamics in gels

Next, Fig. 5(a) shows $S(Q, \omega)$ for the homo-gel under uniaxial deformation ($\lambda = 1, 2, \text{ and } 3$) at $Q = 0.8 \text{ Å}^{-1}$. The dynamic structure factors were fitted with eqn (1) and the fitting results are shown as dashed lines. As shown in Fig. 5(b), the average



(a)

(b)

[su] <1>

(c)

(d)

Fig. 5 (a) Dynamic structure factor $S(Q, \omega)$ of the homo-gel. The dashed

Fig. 6(a) shows $S(Q, \omega)$ for the hetero-gel under uniaxial deformation ($\lambda = 1, 2, \text{ and } 3$) at $Q = 0.8 \text{ Å}^{-1}$. A sharp elastic peak corresponding to slow chain dynamics with a broad base was observed under deformation ($\lambda = 2$ and 3), while only a broad peak was seen in the un-deformed state ($\lambda = 1$). This means that the slow chain dynamics appears only for the deformed hetero-gel. Therefore, in these cases, $S(Q, \omega)$ factors were fitted using the following equation with the sum of the KWW function for the relaxation component and delta function for the elastic component:

$$S(Q,\omega) = \left\{ A_1 \delta(\omega) + \mathrm{FT} \left[A_2 \exp\left(-\frac{t}{\tau}\right)^{\beta} \right] \right\} \otimes R(Q,\omega) \quad (3)$$



Fig. 6 (a) Dynamic structure factor $S(Q, \omega)$ of hetero-gel. The solid lines represent the fitting results. *Q* dependence of (b) average relaxation time and (c) stretching exponent β for hetero-gel at $\lambda = 1, 2,$ and 3. (d) Schematic illustration of the deformation mechanism for hetero-gel.

The elastic component can be ascribed to a slow chain dynamics of highly stretched short strands. When the heterogel is stretched, the short strands oriented in the stretching direction are strongly stretched and the chain dynamics of the highly deformed chains is suppressed. Fig. 6(b) and (c) shows the Q dependence of the average relaxation time τ and stretching exponent β for the quasi-elastic component fitted with the KWW function, respectively. The relaxation component corresponds to the dynamics of the rest of the polymer strands except for the highly stretched chains. As shown in Fig. 6(b), although the average relaxation time becomes shorter with stretching, the extension ratio dependence of the average relaxation time for the hetero-gel is weaker than that for the homo-gel (Fig. 5(b)). The weak dependence of the relaxation time suggests that the stress/strain concentration on some short strands in the hetero-gel relaxes the local deformation of the other polymer strands mainly composed of long chains (Fig. 6(d)). As shown in Fig. 6(c), β of the QENS component is almost independent of λ , which means that the relatively relaxed strands are deformed uniformly with stretching. The average fraction of the elastic component, $A_1/(A_1 + A_2)$ is 1.4% for $\lambda = 2$ and 3 within the measured Q range, which is less than the fraction of proton number of the short pre-polymer PTE-50PA, 12.5%. This result suggests that the stress concentration occurs on about 11% monomers of the short strands in hetero-gel.

4. Conclusion

In this work, we investigated the segmental and monomer dynamics in homogeneous and heterogeneous tetra-PEG gels (homo-gel and hetero-gel) by QENS. Compared with the tetra-PEG solutions, the un-deformed tetra-PEG gels show about the same segmental and monomer dynamics. While the heterogeneity of the polymer networks does not influence the local chain dynamics in the un-deformed state, the inhomogeneity of the network structure is crucial for the local chain dynamics under stretching. The hetero-gel under stretching exhibits a small elastic peak corresponding to the slow dynamics of highly stretched short strands, while for the homo-gel, only a broad quasi-elastic component was observed. The existence of the highly stretched strands results in the smaller strain/stress at break for the heterogeneous gels. QENS measurements on deformed polymer gels and elastomers are quite useful to detect stress concentrations in the materials and deepen the understanding of the fracture mechanism.

Conflicts of interest

There are no conflicts to declare.

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